



Ion Beam Imaging Activities at TU Wien and HEPHY

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MedAustron in a Nutshell



- Ion therapy centre for cancer treatment
 - Synchrotron accelerator complex located close to Vienna
 - Four irradiation rooms:
 - IR1: Exclusive to research (up to 800 MeV protons, low flux)
 - IR2, IR3, IR4: Clinical use (up to 250 MeV protons, GHz rates)
 - Beam delivery only in one room at a time
- Beam parameters for IR1
 - Protons: 60 MeV to 800 MeV
 - Carbon lons: 120 MeV/n to 400 MeV/n
 - Helium: potential upgrade
 - Particle rates: kHz to GHz
- In operation since end of 2016
 - Carbons since mid 2019



MedAustron accelerator complex



IR1 reserved for research

Overview and Outline



- Joint HEPHY/TU Wien working group for Ion Imaging established in 2017
 - Started with 1 PostDoc and 1 Master Student
 - Now 1.5 PostDoc, 3 PhDs, plus students and HEPHY staff support
- Hardware Part I: Existing detector setup and results
 - First prototype based on Belle II tracker prototype sensors plus former TERA range telescope
 - Performance results and limitations presented in this talk
- Software Part I: Reconstruction
 - First trials with TIGRE framework and OS SART reconstruction
- Software Part II: Detector simulation
 - Establish requirements and guidance for hardware design choices
- Hardware Part II: Future directions



Hardware Part I: The Present

Current pCT Setup





- Rotation table to mount object
- Event synchronisation via AIDA2020 trigger logic unit (TLU)

Tracker: Double Sided Si Strips



- Double sided silicon strip sensors
 - > 3+3 planes of ~ $2.5 \times 5 \text{ cm}^2$ each
 - Thickness 300 µm thick
 - X side: 512 n-doped strips, 50 µm pitch
 - Y side: 512 p-doped strips, 100 µm pitch
 - Sensors based on Belle II prototypes
 - APV25 ASIC [1]
 - Belle-II SVD readout chain [2]
- Pros:
 - Low material budget
- Limitations:
 - VME based backend limits us to ~ 500 Hz
 - GbE readout implementation ongoing (independent of pCT activities)
 - Sensors limited in size







Existing DSSD tracker



- Range telescope based on 3 mm thick plastic scintillators read by SiPM
 - Formerly TERA
 - 42 layers of 3 x 300 x 300 mm³ each
 - Can measure protons up to 140 MeV
- Pros:
 - Cheap
 - Can sustain 1 MHz particle rate -> quite ok for prototyping
- Limitations:
 - Dynamic range with 400 pixels per SiPM small -> E_{res} per plane only ~ 8%
 - Accurate energy calibration has proven challenging
 - This thing is old and has seen some wear and tear ...



Existing TERA calorimeter

Selected Results



- No full pCT image up to now
 - Recently managed to calibrate the calorimeter and record correct proton range values
 - If no further roadblocks we should be able to record our first pCT in autumn
- Meanwhile only multiple Coulomb scattering results



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Need new hardware developments!



Software Part I: Reconstruction

TIGRE framework



- TIGRE: Tomographic iterative GPU-based reconstruction toolkit [3]
 - Framework developed for cone-beam CT with contributions from our colleagues at Medical University of Vienna
 - Open source MATLAB/CUDA framework
 - Iterative and direct algorithms implemented (OS-SART was used)
 - Should perform well at limited data sets
- First attempt to adapt the framework to pCT
 - Straight-line approximation
 - Bragg-Kleeman rule



Simulated Setup



- Geant4 simulation of our experimental setup
 - 'Idealised' with perfect spatial and energy resolution per plane
 - 'Realistic' with resolutions matching existing hardware
 - \Box $\sigma_E = 8\%$ per plane
 - σ_x = 14.4 μm
 - σ_y = 28.9 μm



Setup for testbeam validation

Setup for ideal simulation

Reconstruction Results I



- Small phantom: aluminium staircase
 - Idealised and realistic simulation
 - Einit = 100.4 MeV
 - N = 800 primary particles mm⁻²
- Works well but phantom is very small



Real world counterpart



Reconstructed from 'realistic' simulation

Reconstructed from 'idealised' simulation

Reconstruction Results II



- Large phantom: Catphan
 - Idealised simulation only so far
 - Einit = 200 MeV
 - N = 800 primary particles mm⁻² (after cuts)
- Spatial resolution due to straight line approach is clearly limited
 - Cuts on proton paths to improve the spatial resolution amount to data loss
 - MLP has to be added to the framework for further improvement
- Nearly identical results for 180 and 90 projections
- Next step: Integrate MLP in TIGRE
 - Use RTK with distance driven binning as reference

(Thanks to Simon, Nils and Feriel)



Reconstructed from 'idealised' simulation



Software Part II: Design Studies for Future Developments

Guidance for Hardware Design



- Future hardware developments needs comprehensive understanding of uncertainty sources
 - Set detector requirements
 - Guide the design choices
- Geant4 based analysis with many free parameters
 - Single particle tracking setup
 - > Detector: material budget ε and position resolution σ_{p}
 - Geometry: number of planes, distance D, clearance C and thickness T
 - Beam: initial energy E₀ and particle species (proton, helium)
 - > Path model: straight line fit or general broken lines (GBL) in air, most likely path (MLP) in phantom



Overview



- Workflow and Figure-of-Merit
 - Track reconstruction in up- and downstream detectors
 - > 3σ cuts on scattering angle and energy loss
 - Find phantom entry and exit coordinates and direction
 - Reconstruct most likely path (MLP) in phantom
 - Root-mean-square deviation (RMSD) of lateral MLP position at every depth in phantom
 - Max. RMSD along phantom depth is converted to spatial frequency and minimum voxel size







- Iso-voxel spacing in [mm] for phantom thickness T = 20 cm, detector distance D = 10 cm
- With small air gap, lower limit in voxel spacing is ≈ 0.75 mm
- For a voxel spacing \leq 2 mm and 300 mm clearance, material budget should be below
 - > 0.25% per plane, at $\sigma_p = 200 \ \mu m$
 - > 0.70% per plane, at $\sigma_p = 50 \ \mu m$





- Iso-voxel spacing in [mm] for phantom thickness T = 20 cm, detector distance D = 10 cm
- Material budget influence ≈ half as large compared to protons
- A lower limit in voxel spacing is just below 0.5 mm
- 2 mm more easily achieved

Number of Detector Planes





- Test 2+2 planes vs. 3+3 planes with straight line fit and general broken line fit (GBL)
 - > For protons and straight line fits, six planes is worse, due to increased downstream scattering
 - > For helium, six planes is slightly better, due to reduced upstream angular confusion
- 3 plane GBL performs slightly better than four plane straight line fits
 - Doesn't justify additional investment and integration effort of 2 more planes



Hardware Part II: The Future

Time-of-Flight based Ion CT



- In the past few years time resolutions down to
 30 ps have become accessible
 - Strong interest from HEP community
- Technology of Low Gain Avalanche Detectors (LGADs)
 - Allow tracking in time and space
 - Low material budgets
- Energy measurement via ToF competitive in this energy regime
 - With 4 planes á 50 ps, σ_E~1.9% @ 150 MeV
 - With 4 planes á 30 ps, σ_E~1.2% @ 150 MeV
- Several advantages
 - Simplifies the detector layout
 - Flexible measurement over a large energy range



Energy resolution with 2+2 planes at various time resolutions and 1m flight path [Geant4 Sim]

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LGADs in a Nutshell

- Thin silicon pad detectors with gain of ~10
 - Additional high p-doped gain layer in n-in-p diode to create field in excess of 200 kV/cm
 - Controlled impact multiplication
- Gain boosts S/N and improves time resolution
 - Jitter term dominated by trise and S/N
 - Constant term dominated by Landau noise, synchronisation between channels and TDC







Three Possible Setups



- Option 1: Use TOF only for E-ΔE measurement
 - Tracker can use a different technology like depleted CMOS
 - **Modest requirements** of $\sigma_{\text{spatial}} \sim 1 \text{ mm}$, high fill factor easily achieved
 - Can deliver a relatively low cost and flexible calorimeter option



Sketch of TOF E- Δ E setup with separate pixel trackers

Three Possible Setups



2nd TOF Station

- Option 2: Extend rear tracker based on LGADs over a suitable distance
 - Front tracker can still use a different technology
 - Stricter requirements on $\sigma_{spatial}$ and fill factor
 - Sketch assumes LGAD strip sensors



Sketch of TOF rear tracker setup with pixel front trackers

Three Possible Setups



- Option 3: Build a full 4D tracking system
 - Front tracker is also based on LGAD technology
 - **Challenging requirements** $\sigma_{spatial} < 0.1$ mm, high fill factor difficult
 - Reduces development effort by almost a factor ~2
 - > Allows to access the TOF through the body which can be used for e.g. filtering in HeCT [4]



What is needed for Realisation?



- Construction site I: The **sensor**
 - **★** Need strip geometry with pitch < 150 μ m for spatial resolution (< 1 mm for E- Δ E detector)
 - HADES T0 group has demonstrated 47 ps with 146 μm pitch and NINO ASIC [5]
 - ★ Need fill factor > 95% is needed to avoid a third detector layer
 - FBK has demonstrated **trench isolated LGADs** with 7 µm no-gain area [6]
- Construction site II: The **ASIC**
 - ★ Need a fully integrated multi-channel ASIC with amplifier, discriminator and digitisation @ rates of at least O(100 kHz per channel) in data driven readout
 - Can be achieved by adaptation of existing ASICs
 - Suitable analog and digital front-end parts exist already [e.g. 7,8]
- Construction site III: Low mass, tile-able module design
 - Need low material budget < 0.7% X₀ per plane for 4D tracker option (< 1.5% X₀ for E-ΔE option)
 - Can be done via **adaption from existing designs** e.g. from Belle II SVD
 - Integrated ASIC including TDC is essential to create a tile-able design for e.g. 30 x 30 cm²

Test Beam Setup

- Sensors: Single diodes
 - FBK UFSD2 production
 - Sensitive area 1x1 mm²
- Frontend: UCSB single LGAD board
 - 1st amplification stage: Infineon BFR840 SiGe
 - > 2nd amplification stage: Not needed!
 - Two boards back to back with 2.5 cm spacing
- Backend: Tektronix Oscilloscope 25GS/s and 8 GHz BW
 - Diodes have intrinsic rise time of ca. 500 ps
 - Operation at 1 GHz has shown best S/N values
- Offline: Waveform analysis
 - Rising edge fit to extract timestamp at CF=30%
 - RMS of the time difference between two planes





test beam setup



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Selected Results

- Time resolutions of around 50ps (40ps) achieved for protons (carbons)
 - Improvements towards lower E_{beam} due to higher E_{dep} and better S/N
 - Not quite the expected 30 ps
 - 8bit dynamic range of oscilloscope not ideal
 - Shielding and temperature control might further improve









- Joined HEPHY/TU Wien working group for Ion Imaging has been established
 - Goal is to establish an ion CT setup at MedAustron
- Existing hardware has shown strong limitations
 - Setup based on double-sided silicon strip sensors and range telescope finally working
 - Not suitable for the future
- TIGRE framework using iterative reconstruction is being investigated
 - Currently lacks MLP implementation but appears promising at reduced N_{projections}
- New developments towards time-of-flight based system have started
 - Simulation to guide new hardware developments
 - Cooperation with interested partners (FBK, GSI, TU Darmstadt and CREATIS) has been established
 - Currently looking for funding



- [1] M. J. French et al. 2001, <u>https://doi.org/10.1016/S0168-9002(01)00589-7</u>
- [2] R. Thalmeier et al. 2017, <u>https://doi.org/10.1016/j.nima.2016.05.104</u>
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- [4] M. Rovituso et al. 2017, <u>https://doi.org/10.1088/1361-6560/aa5302</u>
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Backup

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Cancer treatment with ion irradiation

- Cause cellular damage
- Either via direct ionisation of DNA molecules or indirect via creation of free chemical radicals

Ion Therapy in a Nutshell

- Ion beams allow for a strongly localised energy deposition
 - More accurate dose profile compared to photons
 - Allows treatment of tumours close to radiosensitive tissue, e.g. optical nerve
- Two therapies: Protons and heavier ions
 - Protons allow for sharp distal edge
 - Heavier ions have higher biological effectiveness (RBE) but show a tail dose due to fragmentation
 - Different ions used for different tumours



dose deposition in water [GATE simulation]



MedAustron Accelerator





MedAustron Timeline





Imaging with Ion Beams



- Aim: 3D map of stopping power within object
 - Requires ΔE and path estimate
- Particles with energy E
 - Pass front tracker
 - Lose energy ΔE in object
 - Pass rear tracker
 - Deposit energy E-ΔE in calorimeter
- Ion CT
 - Measure ΔE and path estimate
 - Rotate object and reconstruct
 - > 3D map of stopping power within object
 - Avoids conversion uncertainties from photon attenuation coefficients (x-ray CT) to stopping power (ion therapy)

Same particle species for treatment and imaging



pCT setup sketch

Requirements Spatial resolution of about 1x1x1 mm³ (typical voxel size) in the object

- Energy resolution of about 1%
- Data acquisition rate of >1 MHz
- Rad hard to ~1e13 protons over 10 years of operation
- Coverage >10x10 cm²
- Typical Setup
 - Front and rear tracker
 - Scintillating fibres or Si-strip
 - Energy measurement
 - Crystal calorimeter: Csl, YAG:Ce
 - Range counter: stack of thin detector layers made of scintillators or CMOS
 - Time-of-flight measurement

An Apparatus for Ion CT





pCT setup sketch

LGADs for Ion CT



Excellent time resolution

- Time resolutions of 30 ps envisaged for CMS/ ATLAS timing layer for single MIPs
- Energy deposition in relevant beam range is several MIPs
- Energy deposition of heavy ions is less 'Landaulike' and could allow for a reduced Landau noise
- Good radiation hardness
 - Radiation hardness shown to above 1e15
- Could render rear tracker unnecessary
 - Required precision driven by MCS limit and varies with object length
 - Spatial resolution of below 1 mm achievable with current LGAD designs
 - Significant efforts for further improvements



