Development of iterative image reconstruction for track-based multiple scattering computed tomography using a high-energy electron beam

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Introduction

- Computed Tomography
 - Absorption: Photon (X-ray), neutron, muon, …
 - Energy loss: Proton, …
 - Multiple Coulomb Scattering (MCS) with high energy electron
 - Gaussian width of the deflection angle distribution: (Highland's approximation of the Moliere's theory)



Material Budget Imaging (MBI) with MCS Page: 3

Track-based multiple scattering tomography



- Measure the hit positions of individual electrons on sensor planes upstream and downstream of the sample under test (SUT)
- Reconstruct the tracks and calculate the scattering angle (k_{x,y})
- We use absolute deviation of the distribution's inner 90% quantile (<u>AAD₉₀</u>) to calculate Θ₀

Potentials of Material Budget Imaging

- Potentials
 - Non-destructive imaging of <u>high-Z</u> materials
 [>1 GeV electron]
 - Medical imaging for treatment planning [O(100) MeV electron]
 - Low dose, better spatial/density resolution, less metal artifacts
- Challenges
 - Statistics: high rate data acquisition and beam rate
 - Detector size

Test beam Experiment at DESY

Hamburg-Bahrenfeld





- We performed test beam experiment on June 2020
- Independent electron beam at DESY II synchrotron
- User selectable energy: O(100) MeV ~ 6 GeV

EUDET-type Telescope





- 6 silicon pixel sensors (MIMOSA26)
 - Pitch: 18.4 μ m × 18.4 μ m
 - Area: 10.6 mm × 21.2 mm
 - Intrinsic sensor resolution: > 3.24 μ m
- 4 PMTs for coincidence trigger

2D Material Budget Imaging



- SUT: small Lithium-ion battery
- The AAD² distribution shows the fine inner structure of the battery

Electron CT



Reconstruction



(Ref: APPLIED PHYSICS LETTERS 112, 144101)

- Measurement with different rotation angles to create a sinogram
- ► Reconstruction algorithm
 - Filtered back projection (FBP)
- **DESY.** | 3D Material Budget Imaging | Hendrik Jansen | 18.01,2019 - Iterative reconstruction?

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Iterative Image Reconstruction

$$\overrightarrow{y} \longrightarrow \overrightarrow{y} = A \overrightarrow{x} \longrightarrow \overrightarrow{x}$$

$$\overset{\text{Image}}{\underset{\text{Image}}{\underset{\text{(Truth)}}{\text{Image}}}}$$
Suppose that:
$$\overrightarrow{y} = A \overrightarrow{x} + \overrightarrow{n}$$

$$J(\overrightarrow{x}) = ||A\overrightarrow{x} - \overrightarrow{y}||^2$$

$$A^T A \overrightarrow{x} = A^T \overrightarrow{y} \quad (\text{minimize } J(\overrightarrow{x}) \to \partial J(\overrightarrow{x}) / \partial \overrightarrow{x} = 0)$$

Landweber method:

$$\overrightarrow{x}^{(k+1)} = \overrightarrow{x}^{(k)} + \alpha A^{T} (\overrightarrow{y} - A \overrightarrow{x}^{(k)})$$

$$\overrightarrow{x}^{(k+1)} = \overrightarrow{x}^{(k)} + \sum_{i=1}^{I} \alpha \|\overrightarrow{a_{i}}\|^{2} \frac{y_{i} - \overrightarrow{a_{i}} \cdot x_{i}^{(k)}}{\|\overrightarrow{a_{i}}\|^{2}} \overrightarrow{a_{i}}$$

Simultaneous iterative reconstruction technique (SIRT) Page: 10

Projection method

$$\overrightarrow{x}^{(k+1)} = \overrightarrow{x}^{(k)} + \sum_{i=1}^{l} \alpha_{i} \|\overrightarrow{a_{i}}\|^{2} \frac{y_{i} - \overrightarrow{a_{i}} \cdot x_{i}^{(k)}}{\|\overrightarrow{a_{i}}\|^{2}} \overrightarrow{a_{i}}$$

= 1 \rightarrow Algebraic reconstruction technique



SIRT Projection

$$\overrightarrow{x}^{(k+1)} = \overrightarrow{x}^{(k)} + \sum_{i=1}^{I} \alpha \|\overrightarrow{a_i}\|^2 \frac{y_i - \overrightarrow{a_i} \cdot x_i^{(k)}}{\|\overrightarrow{a_i}\|^2} \overrightarrow{a_i}$$

Simultaneous projection with weighting $\sum_{i=1}^{r} \alpha \|\vec{a}_i\|^2$

 α : step size (free parameter)

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Comparison between FBP

- Computing time
 - Concurrent processing in forward/back projection
- Statistical noise (9)
 - Unknown statistical noise of the width (AAD₉₀) of the scattering angle distribution
- Regularization
 - Many variety of the regularization term can be implemented in the iterative algorithm

U(x): energy function

$$\overrightarrow{x}^{(k+1)} = \overrightarrow{x}^{(k)} + \alpha \left[A^T (\overrightarrow{y} - A \overrightarrow{x}^{(k)}) + \beta \frac{\partial U(\overrightarrow{x})}{\partial \overrightarrow{x}} \right]$$

Function: quadratic, gaussian, total variation, \cdots

Alignment Phantom



- 5 iron rods in a half-length plastic cylinder
- Online monitoring was performed to fix the position of the rotation stage
- 360° scan with 0.9° step scan for 3D image reconstruction (= 400 projections)

DESY Logo Phantom



w/ regularization

Preliminary (scale is modified for comparison)



w/o regularization

- 40 iterations
- Regularization reduces the noise
 - Energy function: quadratic (smooth the image)

Quantitative study is on-going! Page: 15

Toward the Electron CT for Medical Imaging

https://www.slideserve.com/taylor/gean4-human-phantom-advanced-example-a-geant4-anthropomorphic-model



- All-pix² simulation framework
 - https://project-allpix-squared.web.cern.ch/project-allpix-squared/
 - Based on Geant4 toolkit
- Study of systematical effect
 - Mechanical misalignment, metal artifacts, most likely path estimation, \cdots
- Feasibility study of medical imaging with O(100) MeV electron
 - Target: Anthropomorphic model with GDML
 - CNR, resolution, dose, \cdots

Conclusions

- Material Budget Imaging/Electron CT has potentials for non-destructive imaging and clinical imaging
- Test beam experiment was performed at DESY in June
- Iterative image reconstruction algorithm was developed for 3D reconstruction
 - Regularization contributes to the noise reduction
- MC simulation has been developed for systematic study and clinical imaging

Any ideas/comments are welcome!



Track reco and width estimation

General Broken Lines (GBL) for track fitting

- Find the most probable trajectory based on the measured hits
- Includes known MB at planes
- Introduces unbiased kink at the sample

Method for width estimation

- Calculate Average Absolute Deviation of the inner 90% quantile
- Best performance out of 11 tested fitting and statistical methods
- Conversion to MB via Highland formula or via calibration

Challenges

- Non-Gaussian tails of the distribution

.

- Low statistics





Comparison to CT

Cross-sections



CT scan at 170 kVp (inverted grey scale)







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3D reconstruction for alignment phantom



- 10 iterations, no regularization
- Artifacts due to the absence of calibration (under study)
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